ORIGINAL ARTICLE



# Thermoresponsive and Biodegradable Amphiphilic Block Copolymers with Pendant Functional Groups

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#### Abstract

**BACKGROUND:** To develop the biodegradability and thermoresponsive hydrogel, in this work we designed a pendant-functionalized, thermoresponsive, amphiphilic block copolymer.

*METHODS:* Methoxy poly(ethylene glycol) (MPEG)-*b*-[poly(ε-caprolactone)-*ran*-poly(ε-caprolactone-3-one)-*ran*-polylactic acid] (MCL) and (MPEG-*b*-[PCL-*ran*-POD-*ran*-PLA]) [MCL-(CO)] block copolymers were prepared by ringopening polymerization of ε-caprolactone, OD and lactide monomers. The subsequent derivatization of MCL-(CO) provided MPEG-*b*-[PCL-*ran*-poly(ε-caprolactone-3-COOH)-*ran*-PLA] [MCL-(COOH)] with COOH pendant groups and MPEG-*b*-[PCL-*ran*-poly(ε-caprolactone-3-NH<sub>2</sub>)-*ran*-PLA] [MCL-(NH<sub>2</sub>)] with NH<sub>2</sub> pendant groups.

**RESULTS:** The measured segment ratios of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) agreed well with the target ratios. The abundances of the COOH and NH<sub>2</sub> groups in the MCL-(COOH) and MCL-(NH<sub>2</sub>) copolymers were determined by <sup>1</sup>H- and <sup>13</sup>C-nuclear magnetic resonance spectroscopy, and agreed well with the target abundances. MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) formed homogeneous, white, opaque emulsions at room temperature. Rheological analysis of the block copolymer suspensions indicated a solution-to-hydrogel phase transition as a function of temperature. The solution-to-hydrogel phase transitions and the biodegradation of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) were affected by varying the type (ketone, COOH, or NH<sub>2</sub>) and abundance of the pendant groups.

*CONCLUSION:* MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) with ketone, COOH, and NH<sub>2</sub> pendant groups showed solution-to-hydrogel phase transitions and biodegradation behaviors that depended on both the type and number of pendant groups.

**Keywords** Thermoresponsive · Amphiphilic block copolymers · Pendant group · Solution-to-hydrogel phase transitions · Biodegradation

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#### 1 Introduction

Recently, several thermoresponsive amphiphilic block copolymers exhibiting solution-to-hydrogel phase transitions, as a function of temperature, have been reported [1, 2]. If amphiphilic block copolymer solutions (as thermoresponsive hydrogel) can be prepared at room temperature, biologics, such as drugs and cells, can easily be mixed into the copolymer [3]. Therefore, various amphiphilic block copolymers have been employed as candidates for use as thermoresponsive polymers [4–10]. The thermal

sition [3]. Recently, several groups, including ours, have reported thermoresponsive amphiphilic block copolymers consisting of poly(ethylene glycol) (PEG) and biodegradable polyesters—such as poly(ɛ-caprolactone) (PCL), polylactic acid (PLA), and polyglycolic acid (PGA) [or their copolymers, such as poly(lactic-co-glycolic acid)] [11-13]. Recently, we prepared amphiphilic block copolymers with functional groups at the chain-end and pendant positions via ringopening copolymerization (ROP) of a 3-benzyloxymethyl-6-methyl-1,4-dioxane-2,5-dione, 2-chloride-*\varepsilon*-caprolactone, or 4-benzyloxy-ε-caprolactone, monomer with εcaprolactone (CL), glycolide (GA), or L-lactide (LA); we then measured the thermal response as a function of temperature [14–19]. The pendant functional groups on the amphiphilic block copolymers altered the formation of

domains; this causes the solution-to-hydrogel phase tran-

Scheme 1

coaggregated hydrophobic domains via intra- and intermolecular hydrophobic aggregation.

In this study, to develop a novel, pendant-functionalized, thermoresponsive, amphiphilic block copolymer, we prepared the 2-oxepane-1,5-dione (OD) monomer (Fig. 1) [20]. CL, OD, and LA monomers were co-polymerized with methoxy poly(ethylene glycol) (MPEG) in various ratios to MPEG-b-[PCL-ran-poly(ɛ-caprolactone-3-one)prepare ran-PLA] [MCL-(CO)] block copolymers. MPEG-b-[PCLran-poly(ɛ-caprolactone-3-COOH)-ran-PLA] [MCL-(COOH)] and MPEG-b-[PCL-ran-poly(ɛ-caprolactone-3-NH<sub>2</sub>)-ran-PLA] [MCL-(NH<sub>2</sub>)] were prepared by the subsequent derivatization of MCL-(CO). We measured the thermal responses of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) with ketone, COOH, and NH<sub>2</sub> pendant groups. Finally, we examined the biodegradability of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>). Thus, we investigated the solution-to-hydrogel phase transitions and biodegradabilities of MCL-(CO), MCL-(COOH), and



Fig. 1 Synthesis of 2-oxepane-1,5-dione (OD) (Scheme 1) and preparation of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers (Scheme 2)

MCL-(NH<sub>2</sub>) with different species and numbers of pendant groups.

#### 2 Experimental

#### 2.1 Materials

MPEG (number-average molecular weight,  $M_n$ , = 750; Sigma, MO, USA), tin(II) 2-ethylhexanoate (Sn(Oct)<sub>2</sub>; Sigma, MO, USA), 1,4-cyclohexanedione (Sigma, Mo, USA), *meta*-chloroperoxybenzoic acid (*m*CPBA; Sigma, MO, USA), carboxymethoxylamine hemihydrochloride (TCI, Tokyo, Japan), *p*-toluenesulfonic acid monohydrate (*p*TSA; TCI, Tokyo, Japan), *N*-hydroxysuccinimide (NHS; Sigma, MO, USA), *N*,*N'*-dicyclohexylcarbodiimide (DCC; Sigma, MO, USA), and diaminobutane (Sigma, MO, USA) were used as received. CL (TCI, Tokyo, Japan) was distilled over CaH<sub>2</sub> under reduced pressure prior to use. LA (Boehringer Ingelheim, Germany) was recrystallized twice from ethyl acetate prior to use. Dichloromethane (DCM) was distilled sequentially, under nitrogen, over CaCl<sub>2</sub> and CaH<sub>2</sub>, before use.

#### 2.2 Characterization

<sup>1</sup>H- and <sup>13</sup>C-nuclear magnetic resonance (NMR) spectra were measured using a Mercury Plus 400 spectrometer (Varian); CDCl<sub>3</sub> and D<sub>2</sub>O were used as solvents and tetramethylsilane as the internal standard. The molecularweight distributions of each copolymer were measured at 40 °C using a Futecs gel permeation chromatograph (GPC; RI-201H, refractive index detector) and polystyrene gel columns (Shodex K-802, K-803 and K-804). CHCl<sub>3</sub> was used as the eluent at a flow rate of 1.0 mL/min. Polystyrene was used as the calibration standard. The hydrodynamic diameters of the particles formed from each copolymer were measured by dynamic light scattering (DLS; ELSZ-1000, Otsuka Electronics, Osaka, Japan) at room temperature.

#### 2.3 Preparation of 2-oxepane-1,5-dione (OD)

Prior to use, all glassware was dried by heating under vacuum and then flushed with dry nitrogen. All reactions were conducted under dry nitrogen. First, 1,4-cyclohexanedione (5.00 g, 43.80 mmol) was dissolved in DCM (200 mL) and stirred for 2 h at 50 °C. Then, *meta*chloroperoxybenzoic acid (10.60 g, 61.33 mmol) in DCM (60 mL) was added to the solution dropwise and the mixture was stirred at 25 °C. After 15 h, the solution was concentrated by rotary evaporation of the DCM. The reaction mixture was then washed thrice with diethyl ether. The organic phase was extracted and the solvent removed by evaporation, yielding a white power (OD) (2.69 g, 20.99 mmol, 48% yield). <sup>1</sup>H-NMR (CDCl<sub>3</sub>): 4.41 (t, 2H, –  $CH_2O$ )–), 2.83 (t, 2H, – $CH_2$ –COO–), 2.74 (m, 4H, – $CH_2$ -CO–). Elemental analysis results: abundances calculated for C<sub>6</sub>H<sub>8</sub>O<sub>3</sub>: C: 56.24, H: 6.29; measured: C: 55.95, H: 6.28.

# 2.4 Synthesis of MPEG-*b*-[poly(ε-caprolactone)ran-poly(L-lactide)] (PCL-ran-PLA) diblock copolymer (MCL)

A solution of MPEG (1 g, 1.33 mmol) in toluene (65 mL) was azeotropically distilled to remove the water present in the MPEG; around 30 mL of toluene was removed. CL (2.81 g, 24.59 mmol) and LA (0.39 g, 2.71 mmol) were added to the solution. These were followed by Sn(Oct)<sub>2</sub> in dry toluene (1.6 mL, 0.1 M), which was added to the solution at 25 °C, under a nitrogen atmosphere. After polymerization for 24 h at 130 °C, the reaction solution was added to a mixture of *n*-hexane and diethyl ether (v/ v = 4/1) to precipitate MCL. The precipitated polymer was removed from the solution by filtration and dried under vacuum to yield a colorless solid.

### 2.5 Synthesis of MPEG-*b*-[PCL-*ran*-poly(εcaprolactone-3-one)-*ran*-PLA] [MCL-(CO)]

Prior to use, all glassware was dried by heating under vacuum and then flushed with dry nitrogen. A typical polymerization process, used to synthesize MCL-(CO)<sub>10</sub> with a CL:OD:LA ratio of 80:10:10 and using MPEG as an initiator, was as follows: A mixture of MPEG (1.88 g, 2.50 mmol) and toluene (65 mL) was azeotropically distilled to remove any water; around 30 mL of toluene was removed. CL (4.63 g, 40.56 mmol), OD (0.65 g, 5.07 mmol), and LA (0.73 g, 5.06 mmol) were added to the solution. These were followed by  $Sn(Oct)_2$  in dry toluene (3 mL, 0.1 M), which was added at 25 °C under a nitrogen atmosphere. After polymerization for 24 h at 130 °C, the reaction solution was added to a mixture of nhexane and diethyl ether (v/v = 4/1) to precipitate MCL- $(CO)_{10}$ . The obtained MCL- $(CO)_{10}$  was dissolved in DCM. The resultant solution was reprecipitated to cold methanol. MCL-(CO)<sub>3</sub>, MCL-(CO)<sub>5</sub>, and MCL-(CO)<sub>15</sub> with molecular weights of 2400 g/mol were prepared according to the same protocol. The ratio of the poly(CL), poly(OD), and poly(LA) segments in the MCL-(CO) copolymers was determined by comparing the intensity of the carbonyl peaks at 173.8 ppm, 198.1 ppm, and 170.2 ppm (poly(CL), poly(OD), and poly(LA), respectively) in the  $^{13}$ C-NMR.

# 2.6 Synthesis of MPEG-*b*-[PCL-*ran*-poly(εcaprolactone-3-COOH)-*ran*-PLA] [MCL-(COOH)]

MCL-(CO)<sub>10</sub> (4 g, 1.27 mmol), carboxymethoxylamine hemihydrochloride (0.03 g, 0.29 mmol) and *p*-toluenesulfonic acid (15 mg, 0.09 mmol) were dissolved in anhydrous THF (40 mL) and stirred under nitrogen for 4 h at 25 °C. To precipitate MCL-(COOH)<sub>10</sub>, the reaction solution was added to a mixture of *n*-hexane and ethyl ether (v/ v = 4/1). MCL-(COOH)<sub>3</sub>, MCL-(COOH)<sub>5</sub>, and MCL-(COOH)<sub>15</sub> were synthesized according to the same procedure.

# 2.7 Synthesis of MPEG-*b*-[PCL-*ran*-poly(εcaprolactone-3-NH<sub>2</sub>)-*ran*-PLA] [MCL-(NH<sub>2</sub>)]

MCL-(COOH)<sub>10</sub> (3 g, 0.90 mmol) was dissolved in anhydrous DCM (25 mL). *N*,*N'*-dicyclohexylcarbodiimide (0.04 g, 0.21 mmol) and *N*-hydroxysuccinimide (0.02 g, 0.21 mmol) were added to the MCL-(COOH)<sub>10</sub> solution; the mixture was stirred for 6 h at 25 °C and then filtered. Diaminobutane (0.04 g, 0.45 mmol) was added to the solution, which was then stirred for 24 h at 25 °C. The reaction solution was precipitated by adding it to a mixture of *n*-hexane, diethyl ether, and methanol (v/v = 8/1.5/0.5; 1 L). The precipitated mixture was solubilized in DCM and washed three times with distilled water (DW). The organic phase was extracted, dried over anhydrous MgSO<sub>4</sub> and the solvent was removed by evaporation to obtain MCL-(NH<sub>2</sub>)<sub>10</sub>. MCL-(NH<sub>2</sub>)<sub>3</sub>, MCL-(NH<sub>2</sub>)<sub>5</sub>, and MCL-(NH<sub>2</sub>)<sub>15</sub> were prepared according to the same procedure.

# 2.8 Determination of sol-to-gel phase-transition via rheological measurement

The viscosities of the MCL, MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymer emulsions (40 mg in 160  $\mu$ L of DW) were measured using a DV-III Ultra viscometer equipped with a programmable rheometer (Brookfield Engineering Laboratories, Middleboro, MA, USA) and a TC-502P circulating bath with a programmable controller (Brookfield Engineering Laboratories, Middleboro, MA, USA). Using a T-F spindle (Brookfield Engineering Laboratories, Middleboro, MA, USA) rotating at 0.2 rpm, the viscosity of each copolymer emulsion was measured at temperatures from 10 to 50 °C in 1 °C increments.

#### 2.9 In vitro degradation test

Aqueous solutions, with concentrations of 1 wt%, of each copolymer were prepared at 80 °C. These were incubated at 37 °C, with shaking at 100 rpm, for 1, 2 and 4 weeks.

After the specified incubation time, the solutions were freeze-dried. Immediately after lyophilization, the molecular weights were measured by GPC, and compared to those of the unincubated copolymers.

# **3** Results and discussion

#### 3.1 Preparation of 2-oxepane-1,5-dione (OD)

The synthesis of OD was performed according to Fig. 1 (Scheme 1). The ketone, 1,4-cyclohexanedione, was oxidized to its ester (Baeyer–Villiger oxidation) by *m*CPBA. The yield was 48% and the structure was confirmed by <sup>1</sup>H-NMR and elemental analysis (see Scheme 2).

# 3.2 Preparation of MCL, MCL-(CO), MCL-(COOH) and MCL-(NH<sub>2</sub>) copolymers

We have previously reported the preparation of MCL copolymers and studied the effect of the CL:LA ratio on their thermal response [11]. MCL copolymers with a CL:LA ratio of less than 90:10 were almost water-soluble; they showed no phase transition at body temperature (ca. 37 °C), but did show a phase transition to a reduced-viscosity phase above 40 °C. Thus, in this study, we synthesized MCL copolymers with a fixed ratio of [CL + OD]:LA of 90:10, while varying the CL:OD ratio; we also synthesized polyester segments of the same molecular weight (2400 g/mol).

MCL-(CO) was synthesized by ROP with various ratios of CL:OD (Fig. 1, Scheme 2). MCL with a CL:LA ratio of 90:10 was prepared as a control sample. The properties of the MCL and MCL-(CO) copolymers with different CL:OD ratios are summarized in Table 1.

The colorless MCL-(CO) copolymers were obtained with yields of over 90%. All the MCL-(CO) copolymers exhibited a monomodal GPC curve. <sup>1</sup>H- and <sup>13</sup>C-NMR analyses of the MCL-(CO) copolymers showed the characteristic peaks of MPEG, poly(CL), poly(OD), and poly(LA) (Figs. 2, 3). <sup>13</sup>C-NMR signals corresponding to the carbonyl groups of poly(CL), poly(OD), and poly(LA) were observed at 173.8 ppm, 198.1 ppm, and 170.2 ppm, respectively. The CL:OD ratios calculated from the protonand carbon-integration agreed well with the targeted values.

The molecular weights, CL:OD ratios, and [CL + OD]/LA:MPEG ratios of the samples are summarized in Table 1. The MCL-(CO) copolymers exhibited the targeted molecular weights, around 2400 g/mol, and feed ratios of [CL + OD]:LA, as determined from the <sup>1</sup>H- and <sup>13</sup>C-NMR spectra. This indicates that the ROP of CL, OD, and LA

Table 1 Properties of MCL, MCL-(CO), MCL-(COOH) and MCL-(NH<sub>2</sub>) copolymers

Polymer	[CL/OD]/[LA] molar ratio <sup>a</sup> (%)	<i>M</i> <sub>n, calcd</sub> MPEG-polyester	$M_{n, NMR}^{a,b}$ MPEG- polyester	Yield (%)	$M_w/M_n^c$	Hydrodynamic diameter (nm) <sup>d</sup>
MCL	[91/0] [9]	750–2400	750-2390	92	1.31	_
MCL-(CO) <sub>3</sub>		750-2400	750-2470	91	1.53	255
MCL-(COOH) <sub>3</sub>	[91/2] [7]	750-2540	750-2540	92	1.55	324
MCL-(NH <sub>2</sub> ) <sub>3</sub>		750-2610	750-2620	80	1.59	184
MCL-(CO) <sub>5</sub>		750-2400	750-2460	92	1.59	287
MCL-(COOH)5	[89/4] [ <mark>6</mark> ]	750-2600	750-2590	93	1.62	266
MCL-(NH <sub>2</sub> ) <sub>5</sub>		750-2730	750-2730	86	1.63	180
MCL-(CO)10		750-2400	750-2390	93	1.52	332
MCL-(COOH)10	[84/8] [ <mark>8</mark> ]	750-2560	750-2570	89	1.53	215
MCL-(NH <sub>2</sub> ) <sub>10</sub>		750-2740	750-2730	82	1.55	177
MCL-(CO) <sub>15</sub>		750-2400	750-2410	90	1.62	484
MCL-(COOH)15	[83/13] [4]	750-2620	750-2630	91	1.64	196
MCL-(NH <sub>2</sub> ) <sub>15</sub>		750–2850	750–2860	88	1.66	2066

<sup>a</sup>Determined from <sup>13</sup>C-NMR spectra

<sup>b</sup>Determined from <sup>1</sup>H-NMR spectra

<sup>c</sup>Measured by means of gel-permeation chromatography (based on standard polystyrene)

<sup>d</sup>Measured by DLS

yielded the targeted MCL-(CO) copolymers, with ketone group abundance controllable between 3 and 15 mol%.

The MCL-(CO) ketone group was reacted with carboxymethoxylamine to give MCL-(COOH)-MCL with COOH pendant groups. Finally, the MCL-(COOH) copolymer was activated with DCC and NHS and reacted with diaminobutane to give MCL-(NH<sub>2</sub>) copolymers. The MCL-(COOH) and MCL-(NH<sub>2</sub>) copolymers exhibited <sup>1</sup>H NMR peaks characteristic of COOH and NH<sub>2</sub> (Fig. 2). The abundances of the COOH and NH<sub>2</sub> in the MCL-(COOH) and MCL-(NH<sub>2</sub>) copolymers were determined from the  ${}^{1}H$ NMR peaks, and agreed well with the targeted abundances. This indicates that the MCL-(COOH) and MCL-( $NH_2$ ) diblock copolymers contained the targeted abundance of COOH and NH<sub>2</sub> pendant-groups, between 3 and 15 mol% depending on the sample. Collectively, this indicates that the COOH and NH<sub>2</sub> pendant groups were added to the MCL segment with controllable abundances.

# 3.3 Thermoresponsiveness of the MCL, MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymer suspensions

Aqueous solutions of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>), with functional group concentrations between 3 and 15 mol%, were prepared as homogeneous emulsions, which were white and opaque. The control MCL suspension also formed an opaque emulsion. To examine the phase transition behavior of the block copolymer

suspensions, rheological analysis was performed between 10 and 50  $^{\circ}$ C (Fig. 4A).

Below 39 °C, MCL formed a homogeneous solution with a viscosity of 1 cP below; this increased to a maximum of  $4.7 \times 10^3$  cP at 42 °C. The MCL-(CO) copolymer suspensions also exhibited a viscosity of almost 1 cP at low temperatures, indicating a homogeneous suspension due to complete dissolution of the copolymers. With increasing temperature, the viscosity of the MCL-(CO) copolymer suspensions increased until they displayed gel-like behavior. The viscosities and phase-change-onset temperatures of each MCL-(CO) copolymer suspension depended on the functional group content of the sample. The onset temperatures of the MCL-(CO) copolymer suspensions were 33 and 38 °C at 3 and 5 mol% ketone groups, respectively. However, the phase change did not occur with more than 10 mol% ketone groups. The MCL-(CO) copolymer with the highest viscosity was that with 3 mol% ketone groups, at 5.4  $\times$  10<sup>3</sup> cP, which decreased to 2.9  $\times$  10<sup>3</sup> cP at 5 mol%, 950 cP at 10 mol%, and 260 cP at 15 mol%; this indicates that viscosity is inversely correlated with the abundance of the ketone group.

The onset temperatures of the MCL-(COOH) copolymers were 19 and 26 °C for the 3 and 5 mol% COOH pendant groups, respectively (Fig. 4B). The onset temperatures of the MCL-(COOH) copolymers were lower than those of the MCL-(CO) copolymers, but the maximum viscosities were higher. The maximum viscosities of MCL-(COOH) were  $1.3 \times 10^4$  cP and  $9.6 \times 10^3$  cP at 3 and



Fig. 2 <sup>1</sup>H-NMR spectra of A MCL, B MCL-(CO)<sub>10</sub>, C MCL-(COOH)<sub>10</sub> and D MCL-(NH<sub>2</sub>)<sub>10</sub> copolymers in CDCl<sub>3</sub>

5 mol%, respectively. At ketone and COOH pendant group abundances of 3 and 5 mol%, MCL-(COOH) exhibited higher maximum viscosities than MCL-(CO); this is attributed to the intra- and intermolecular hydrogen bonding interactions between the COOH groups.

MCL-(NH<sub>2</sub>) copolymer suspensions showed an onset temperature of 27 °C and a maximum viscosity of  $1.7 \times 10^5$  cP at only 3 mol% (Fig. 4C). The suspensions of the MCL-(NH<sub>2</sub>) copolymers with 5 mol% of pendant group exhibited a viscosity of almost 1 cP at low temperatures, indicating a homogeneous suspended phase due to complete dissolution.

The 3 mol% pendant group samples showed increasing viscosity in the order MCL-(CO)<sub>3</sub>  $\ll$  MCL-(COOH)<sub>3-</sub>  $\ll$  MCL-(NH<sub>2</sub>)<sub>3</sub>. Collectively, the sol-to-gel phase transition of the MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers depended on the type and concentration of the pendant groups. Thus, it is conjectured that the pendant groups on the MCL copolymers affect the stability of the hydrophobic aggregates of MCL copolymers.

# 3.4 Solution properties of the MCL, MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymer suspensions

As the MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers formed homogeneous suspensions, 1 mg/mL copolymer solutions were prepared to compare the solution properties of the different pendant-group-functionalized MCL copolymers.

Figure 5 shows the room-temperature <sup>1</sup>H NMR spectra for the MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers in D<sub>2</sub>O. In D<sub>2</sub>O, the MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers exhibited broad peaks, assignable to the polyester blocks, but, in CDCl<sub>3</sub>, the same copolymers showed narrow resonance peaks (Fig. 2). This is due to limitations on the molecular motion of the polyester blocks when dissolved in D<sub>2</sub>O.

The mean hydrodynamic diameters of the MCL-(CO) copolymer solutions increased as the pendant group abundance increased (Table 1). However, the MCL-



Fig. 3 <sup>13</sup>C-NMR spectra of MCL-(CO), with different amounts of OD, in CDCl<sub>3</sub>

(COOH) and MCL-(NH<sub>2</sub>) copolymer solutions showed a decrease in mean hydrodynamic diameters as the pendant group abundance increased, except in the case of MCL- $(NH_2)_{15}$ .

Collectively, the mean hydrodynamic diameters of the MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers depended on the types and concentrations of the pendant groups. This is attributed to the effects that the pendant groups may have on the formation of MCL micelles.



Fig. 4 Viscosity vs temperature curves of A MCL-(CO), B MCL-(COOH), and C MCL-(NH<sub>2</sub>) copolymers with 3–15 mol% of pendant groups



Fig. 5 <sup>1</sup>H-NMR spectra of A MCL, B MCL-(CO), C MCL-(COOH), and D MCL-(NH<sub>2</sub>) copolymers in D<sub>2</sub>O

# **3.5** Degradation of the MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) copolymers

The copolymer suspensions were stirred to examine, *in vitro*, their degradation behavior in phosphate-buffered saline at 37 °C for 4 weeks. At the end of the process, their molecular weights were measured by GPC. Figure 6A shows GPC traces, recorded at several points throughout the degradation process, for MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>). The remaining molecular weights of MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) versus implantation time were plotted and are shown in Fig. 6B. The GPC traces of the degraded samples show several peaks at higher retention times; the intensity of these peaks increases as a function of time, indicating increasing degradation. Over the degradation process, there is a



Fig. 6 A Gel permeation chromatograms (GPC) charts and **B** the remaining molecular weight versus time for MCL, MCL-(CO), MCL-(COOH) and MCL-( $(NH_2)$  copolymers after 1–4 weeks degradation testing

gradual shift to low-molecular-weight peaks with higher retention times; these are assignable to the degraded species, as the degradation process results in decreases in molecular weight. In this work, the findings indicated that degradation was changed by both the type and number of pendant groups.

#### 4 Conclusions

In this study, we successfully synthesized the thermoresponsive, amphiphilic block copolymers MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>), which have ketone, COOH, and NH<sub>2</sub> pendant groups, respectively. The solution-to-hydrogel phase transition and biodegradation behavior were affected by both the type and number of pendant groups. Although we found that MCL-(CO), MCL-(COOH), and MCL-(NH<sub>2</sub>) can be utilized as potential thermoresponsive materials, further studies will be needed to provide a rationale as drug and as cell delivery carriers in animal model. Additionally, we believe that investigation for biocompatibility of the copolymers will be needed as future work.

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#### Compliance with ethical standards

**Conflict of interests** The authors declare no competing financial interests.

Ethical statement There are no animal experiments carried out for this article.

#### References

- Basu A, Kunduru KR, Doppalapudi S, Domb AJ, Khan W. Poly(lactic acid) based hydrogels. Adv Drug Deliv Rev. 2016;107:192–205.
- Kim DY, Kwon DY, Kwon JS, Kim JH, Min BH, Kim MS. Stimuli-responsive injectable in situ-forming hydrogels for regenerative medicines. Polym Rev. 2015;55:407–52.
- Ramin MA, Latxague L, Sindhu KR, Chassande O, Barthélémy P. Low molecular weight hydrogels derived from urea basedbolaamphiphiles as new injectable biomaterials. Biomaterials. 2017;145:72–80.
- Huang M, Li H, Ke W, Li J, Zhao C, Ge Z. Finely tuned thermoresponsive block copolymer micelles for photothermal effecttriggered efficient cellular internalization. Macromol Biosci. 2016;16:1265–72.
- Zhou T, Li X, Li G, Tian T, Lin S, Shi S, et al. Injectable and thermosensitive TGF-β1-loaded PCEC hydrogel system for in vivo cartilage repair. Sci Rep. 2017;7:10553.

- Song WY, Liu GM, Li J, Luo YG. Bone morphogenetic protein-2 sustained delivery by hydrogels with microspheres repairs rabbit mandibular defects. Tissue Eng Regen Med. 2016;13:750–61.
- 7. Rijal G, Li W. 3D scaffolds in breast cancer research. Biomaterials. 2016;81:135–56.
- Shimojo AAM, Galdames SEM, Perez AGM, Ito TH, Luzo ACM, Santana MHA. In vitro performance of injectable chitosantripolyphosphate scaffolds combined with platelet-rich plasma. Tissue Eng Regen Med. 2016;13:21–30.
- Hsieh FY, Tao L, Wei Y, Hsu SH. A novel biodegradable selfhealing hydrogel to induce blood capillary formation. NPG Asia Mater. 2017;9:e363.
- Kim SK, Cho TH, Han JJ, Kim IS, Park Y, Hwang SJ. Comparative study of BMP-2 alone and combined with VEGF carried by hydrogel for maxillary alveolar bone regeneration. Tissue Eng Regen Med. 2016;13:171–81.
- Kang YM, Lee SH, Lee JY, Son JS, Kim BS, Lee B, et al. A biodegradable, injectable, gel system based on MPEG-*b*-(PCLran-PLLA) diblock copolymers with an adjustable therapeutic window. Biomaterials. 2010;31:2453–60.
- Jang JY, Park SH, Park JH, Lee BK, Yun JH, Lee B, et al. In vivo osteogenic differentiation of human dental pulp stem cells embedded in an injectable in vivo-forming hydrogel. Macromol Biosci. 2016;16:1158–69.
- Kwon JS, Kim SW, Kwon DY, Park SH, Son AR, Kim JH, et al. In vivo osteogenic differentiation of human turbinate mesenchymal stem cells in an injectable in situ-forming hydrogel. Biomaterials. 2014;35:5337–46.

- Kim JI, Kim DY, Kwon DY, Kang HJ, Kim JH, Min BH, et al. An injectable biodegradable temperature-responsive gel with an adjustable persistence window. Biomaterials. 2012;33:2823–34.
- Shim SW, Kwon DY, Park JH, Kim JH, Chun HJ, Koh YJ, et al. Preparation of zwitterionic sulfobetaine end-functionalized poly(ethylene glycol)-b-poly(caprolactone) diblock copolymers and examination of their thermogelling properties. J Polym Sci A Polym Chem. 2014;52:2185–91.
- Lee BK, Park JH, Park SH, Kim JH, Oh SH, Lee SJ, et al. Preparation of pendant group-functionalized diblock copolymers with adjustable thermogelling behavior. Polymers. 2017;9:239.
- Park SH, Kwon JS, Lee BS, Park JH, Lee BK, Yun JH, et al. BMP2-immobilized injectable hydrogel for osteogenic differentiation of human periodontal ligament stem cells. Sci Rep. 2017;7:6603.
- Lee HY, Park SH, Kim JH, Kim MS. Temperature-responsive hydrogels via electrostatic interaction of amphiphilic diblock copolymers with pendant-ion groups. Polym Chem. 2017;8:6606–16.
- Park JH, Park SH, Lee HY, Lee JW, Lee BK, Lee BY, et al. An injectable, electrostatically interacting drug depot for the treatment of rheumatoid arthritis. Biomaterials. 2018;154:86–98.
- Timbart L, Amsden BG. Functionalizable biodegradable photocrosslinked elastomers based on 2-oxepane-1,5-dione. J Polym Sci A Polym Chem. 2008;46:8191–9.